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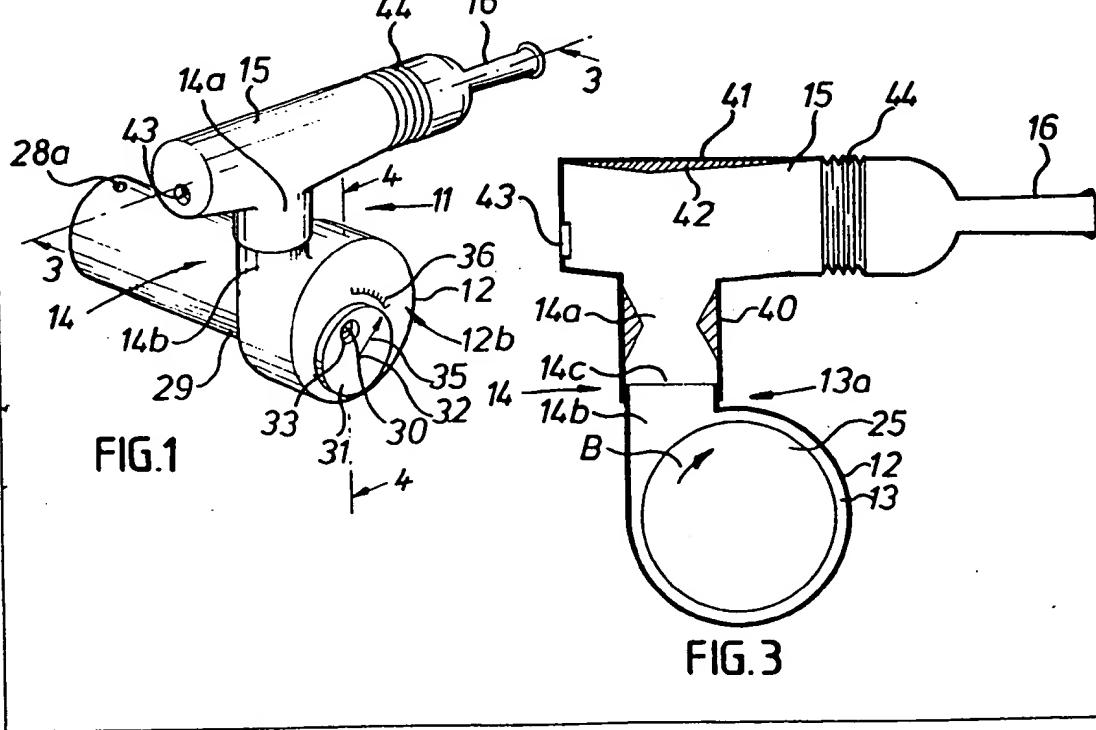
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(54) Nebuliser

(57) The apparatus is self-contained  
 for carriage in a pocket or handbag  
 and comprises a nebulising cham-  
 ber 12 from which tangentially ex-

tends an outlet tube 14 leading to a  
 perpendicular head 15 provided  
 with a mouthpiece 16. The cham-  
 ber is cylindrical and houses a rota-  
 table disc 25. An adjustable air  
 inlet 30 is provided in the chamber  
 and material to be nebulised is in-  
 troduced to the chamber 12  
 through the mouth 14c. The disc  
 25 is driven by a battery and elec-  
 tric motor in the casing 29 and  
 both draws air in through the inlet  
 30 and breaks up the material in  
 the casing to nebulise it. Baffles  
 40, 41 control the size of particles  
 expelled and a damping connection  
 44 reducing unpleasantness to the  
 user from vibrations.



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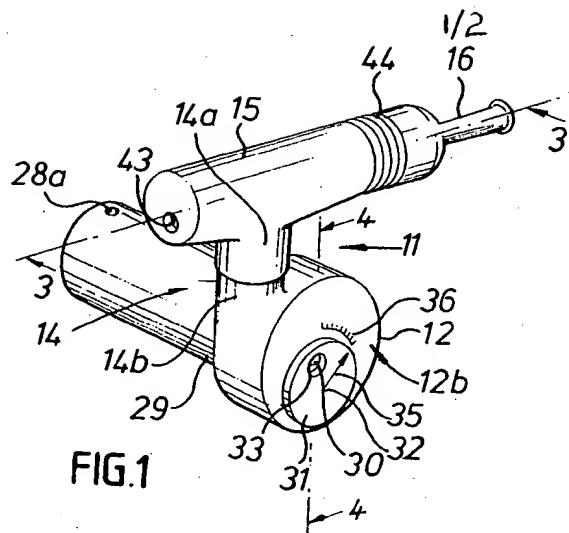


FIG.1

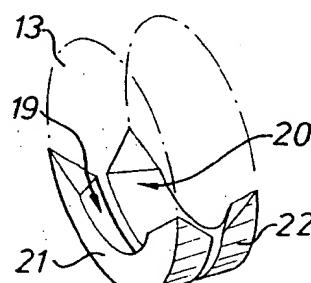


FIG.2

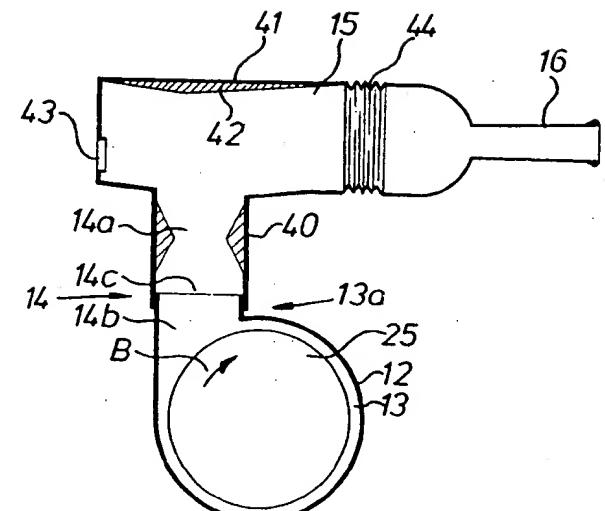


FIG.3

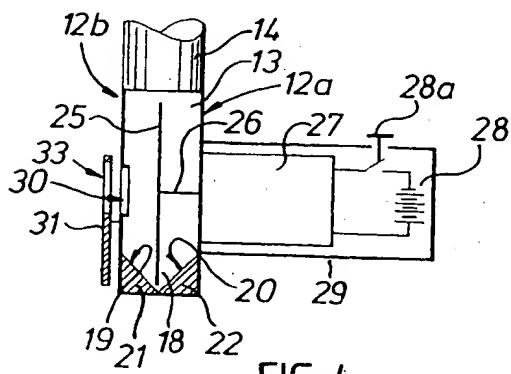


FIG.4

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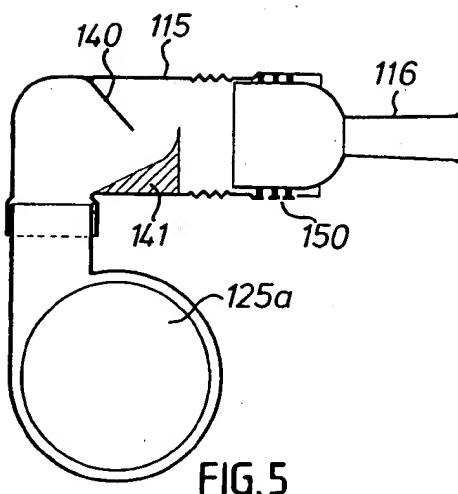


FIG. 5

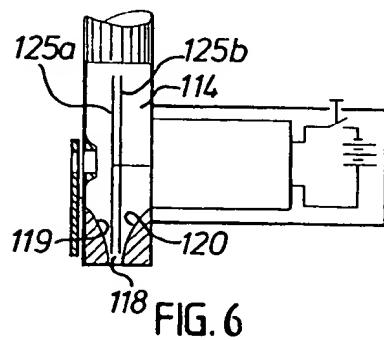


FIG. 6

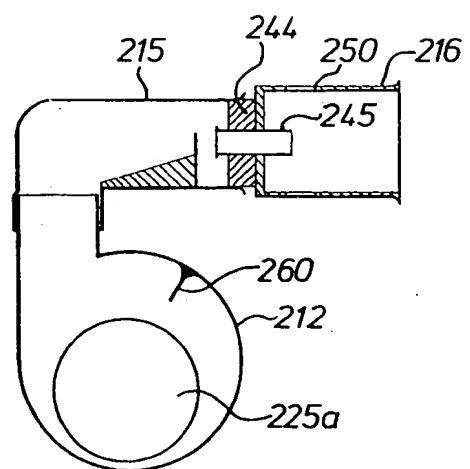


FIG. 7

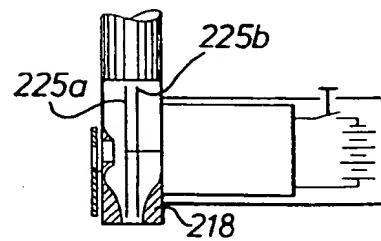


FIG. 8

## SPECIFICATION

## Medical nebulising apparatus

5 The present invention relates to medical nebulising apparatus for inhalatory use. In the specification, the term "nébulisation" is intended to include the formation of a spray from a power as well as from a liquid.

10 In the medical field, the inhalation of nebulised drugs is an accepted way of treating various medical conditions such as asthma, bronchitis, cystic fibrosis and other conditions of the respiratory tract. Existing medical nebulisers are not easy to use by all patients. They are expensive, bulky and require a separate compressed air or oxygen supply, e.g. from a compressed air container or from an electric compressor device. A patient, therefore, is unlikely to have or carry his own nebuliser and has to visit a hospital for inhalation treatment.

25 It has been proposed to use a rotatable disc for dispersing particles in a medical nebuliser. The material is fed in an axial direction onto the disc to disperse the particles in a large chamber and an airstream is independently generated to carry particles out of the chamber. There is generation of a large proportion of large particles and the apparatus is massive.

30 One common way of producing a spray is the pressurised can, commonly used, for example, for such purposes as paint spraying, air fresheners and insecticide sprays. Although these cans are readily portable and are used as inhalation devices, they suffer several drawbacks. They require a pressurised carrier gas, which itself is undesirable for environmental reasons and the pressure is excessively high, with the result that the spray particles impact in the mouth and coalesce. The devices are not re-usable and they need a very high degree of co-ordination and effort by the patient.

35 The present invention provides medical nebulising apparatus, comprising a housing including a chamber provided with a reservoir for material to be nebulised, the housing having an outlet portion for nebulised material, a passage for nebulised material between the chamber and the outlet portion, and nebulising means in the form of a driven rotatable member for effecting nebulisation, characterised in that the rotatable member has its path of rotation passing through the reservoir to pick up material, the passage communicates with the chamber at a port radially spaced from the path of rotation and positioned in the path of particles flung from the rotatable member and the chamber is shaped to direct particles to the port in an air stream centrifugally generated by the rotatable member.

40 The rotatable element is preferably in the form of a rotatable disc and the chamber

45 preferably has a circular peripheral wall about the disc periphery. The passage from the chamber may be tangential to the chamber.

50 The air inlet is preferably an aperture in a wall of the chamber and a shutter may be provided to control the area of the inlet. It is preferred that a scale is provided to indicate the position of the shutter and, therefore, provide predetermined settings for the inlet area. The size of the inlet area determines the rate of delivery of nebulised material by controlling the rate of admission of air to the chamber during operation.

55 The passage between the chamber and the outlet portion preferably includes a baffle arrangement to assist in controlling the particle size at the outlet by returning larger particles to the chamber.

60 Apparatus according to the invention can be made sufficiently small for carrying in a pocket or handbag and can provide a fine mist with particles not exceeding 30 $\mu$  or even as low as 15 $\mu$ .

65 The use of a rotating wheel for flinging particles into a gas stream is a very old practice in some industries, for example, for comminuting metals and electrostatic powder coating. These industrial processes are described in the following U.K. patent specifications, which have been located by searching, since the invention was made.

70 U.K. Patent No. 1,173,380 describes an apparatus for developing electrostatic charge images which involves the use of a disc electrode in an enclosed chamber which dips, while revolving, in a dye liquid. A high voltage is applied to the electrode to cause atomisation of the dye liquid and the atomised particles migrate, by virtue of an applied electrical field, to a conductive support for a recording material carrying a charge image.

75 U.K. Patent No. 1,085,092 describes an apparatus which uses a rotating toothed-disc to direct liquid particles from a reservoir into a gas stream. This apparatus essentially requires a separate supply of gas under pressure to enable the apparatus to function.

80 An apparatus for comminuting molten metal for the purpose of, for example, producing an oxide of that metal is described in U.K. Patent No. 519,784, and a very similar apparatus is described in U.K. Patent No. 574,385. The apparatus of each of these specifications requires a vessel for containing a mass of molten metal and a rotating wheel flings the particles of the molten metal into a gas stream. Specification No. 519,784, which was published forty years ago, does fleetingly, in one sentence, consider that the rotating wheel might serve to produce the gas stream, but for these industrial processes, as for present day medical nebulisers, it is accepted that a separate gas stream-producing apparatus is essential.

85 Reference is now made to the accompany-

ing drawings, wherein:—

Figure 1 is a perspective view of a first embodiment of a medical nebulising apparatus according to the invention;

5 Figure 2 is a perspective view of a broken away portion of the apparatus of Fig. 1 showing a reservoir thereof;

Figure 3 is a sectional side elevation on the line 3-3 of Fig. 1;

10 Figure 4 is a sectional view on the line 4-4 of Fig. 1;

Figures 5 and 6 are sectional views similar to Figs. 3 and 4 of a second embodiment; and

15 Figures 7 and 8 are sectional views similar to Figs. 3 and 4 of a third embodiment.

Referring to Figs. 1 to 4, there is shown a medical nebulising apparatus comprising a housing 11 having a hollow cylindrical portion

20 12 having a chamber 13 therein. An outlet tube 14 leads upwardly (in the position of use shown in Fig. 1) from the cylindrical portion to define an outlet passage tangential to the chamber 13 and communicating therewith

25 through a port 13a. The outlet tube 14 leads to a tubular head 15, which has a T connection with the tube 14. A mouthpiece 16 is connected to one end of the head 15. In use, material to be nebulised is contained in the chamber 12 and a fine spray consisting of an air stream entraining particles of the material is provided at the mouthpiece, as described hereafter.

The lower portion of the chamber 13 opposite to the tube 14 defines a reservoir 18 and internal sloping surfaces 19, 20 cause the reservoir to narrow towards the periphery, each sloping surface being arcuate and following the internal peripheral contour of the

40 chamber as is apparent from Fig. 2. Each surface is defined in this construction by a solid internal wall 21, 22 of substantially triangular section as is apparent from Fig. 4.

A nebulising disc 25 is rotatably mounted 45 in the chamber 13 by an axle 26, so that part of the marginal periphery of the disc lies

between the sloping surfaces 19, 20 in the reservoir, the diameter of the disc being only slightly less than that of the container and the 50 general plane of the disc being parallel to the side walls 12a, 12b of the cylindrical portion 12. The axle is driven by an electrical motor 27 and a replaceable electric battery 28 mounted in a casing 29 on one side wall 12a

55 of the cylindrical portion 12, which defines the chamber 13. A switch 28a is accessible externally of the casing and is actuatable to operate the motor.

The opposite side wall 12b of this portion 60 has a central air inlet 30, the size of which is variable by means of a shutter 31. The shutter in this embodiment is in the form of a disc pivotally mounted by pivot pin 32 on the side wall 12b. The shutter has an aperture 33 of 65 equal diameter to the inlet 30, so that the

inlet is fully open with the aperture 33 and the inlet in register. The shutter can be angularly moved to reduce the area of the inlet exposed. The shutter carries a pointer 35 associated with an arcuate scale 36 marked on the side wall 12b, so that a predetermined area of the inlet can be exposed recording the scale reading.

The outlet parts of the device have an 75 internal baffle arrangement defined by a constriction 40 near the mouth of the outlet tube 14, adjacent the head 15, and a conical projection 41 provided in the head 15 directly opposite the outlet tube 14, the apex 42 of 80 the projection 41 being on the axis of the outlet tube. The end of the head opposite to the mouthpiece 16 is closed except for a vent 43. A flexible bellows 44 attaches the mouthpiece 16 to the head 15.

85 The outlet tube 14 comprises an upper part 14a, integral with the head 15 and a lower part 14b, integral with the cylindrical portion 12. The upper and lower parts are push-fitted together. The head 15, with the upper part

90 14a, can, therefore, be removed, so that the mouth 14c of the lower part defines an inlet.

In use, the material to be nebulised is introduced to the reservoir 18 through the inlet mouth 14c. The patient's mouth is put to 95 the mouthpiece 16 and the electric motor is energised by operating the switch 28a. The nebulising disc 25 is thereby rotated in the direction of arrow B in Fig. 3. A part of the periphery is immersed in the material in the

100 reservoir 18, so that the disc flings particles of the material along the tangential passage in the outlet tube 14. The rotating disc also serves as a centrifugal pump to draw air in through the inlet 30 and produce a gas

105 stream along the passage in the outlet tube, the particles of the material being entrained in the gas stream so that nebulised material passes out of the mouthpiece 16 in a fine spray. The amount of air drawn into the

110 chamber can be controlled by the position of the shutter 31.

As the disc flings particles of the material at a high speed, these particles (especially the larger ones) tend to impact against the inner

115 walls of the chamber 13 and shatter into even smaller particles. The larger particles entering the tube 14 tend to coalesce and drip back into the reservoir 18 or onto the disc for further treatment. This continuous and re-

120 peated action leads to the generation of very small particles. The constriction 40 obstructs flow of larger particles and assists this action as does the conical projection 41 which serves to direct particles which coalesce there

125 back into the reservoir. The spray at the mouthpiece may therefore be made up of particles of maximum size of  $15\mu$ .

The vent permits sucking in of extra air by a patient and also prevents a sucking action at 130 the mouthpiece from drawing in material from

the reservoir and relieves pressure, if the patient obstructs the mouthpiece or blows back into the mouthpiece. The patient can breathe freely, therefore, without interfering with the operation of the apparatus. Venting in this case also prevents wetting of the material in the reservoir from the user's breath, which is important, if the material is a powder.

5 10 The shaping of the reservoir 18 minimises changes in the depth of material therein, with changes in orientation of the apparatus. The disc may be rotationally mounted off-centre or may be unbalanced about the axis

15 20 by other means such as weighting to cause vibrations, which assist in breaking up and fluidising the material in the reservoir to improve nebulisation. This may be especially useful where the material is a powder. Large particles incapable of being nebulised in the apparatus could be contained in the reservoir to cause such vibration and assist in breaking the powder particles into even smaller ones.

These vibrations could cause unpleasant sensations in the lips of the user and the flexible bellows 44 serves to damp the vibrations at the mouthpiece.

25 30 The disc is preferably rotated at 8000 r.p.m. or more to provide a good rate of delivery of nebulised material. The described nebulising apparatus is small and is capable of being held in a pocket or handbag. This is assisted by the connection between the tube parts 14a, 14b, which permits swivelling of the parts to make the apparatus more compact.

35 40 The motor casing 29 may be removable to facilitate sterilisation, unless the casing is watertight. The casing may have, for example, a bayonet or screw fitting with the cylindrical portion 12 and the shaft 26 may have two parts with a spline connection. The battery may be rechargeable from the mains.

An alternative embodiment is shown in

45 50 Figs. 5 and 6, in which the overall construction is substantially the same as the embodiment described above. In this case there are two parallel closely spaced nebulising discs and the internal walls of the reservoir 118 are further spaced at the periphery of the chamber 114 to accommodate the two discs. In this case the walls 119, 120 are convexly curved in section instead of straight.

55 60 Instead of the projection 41 and constriction 40, baffles 140, 141 are provided in the head 115. Ventilation holes 150 are optionally provided in this case adjacent to the mouthpiece 116, the sizing being adjustable by relative movement of the mouthpiece 116 and the rest of the head 115.

Figs. 7 and 8 show a modification of the embodiment of Figs. 5 and 6, in which the nebulising discs are eccentrically positioned relative to the peripheral wall of the chamber

65 and a of smaller diameter than in the previous

ously described embodiment. The discs can be rotated in either direction. The discs are positioned near the bottom of the chamber to extend into the reservoir 218, as previously.

70 75 In this case, a radial baffle 260 is provided in the chamber extending towards the discs. This enhances agitation and disruption of particles within the chamber as a result of impact and also redirects larger particles onto the discs for further treatment.

The mouthpiece 216, in this case is mounted in the outlet from the head 215 by means of a resilient bung 244 to absorb vibrations. An outlet nozzle 245 extends

80 85 through the bung to communicate the interior of the mouthpiece with the interior of the head. Ventilation holes 250 are provided around the mouthpiece. This arrangement is preferred and is particularly effective to permit the user to breathe freely and to prevent air from the lungs of the user reaching the reservoir.

Each of the described embodiments can be easily cleaned and sterilised.

90 95 A very simple arrangement may be effective where the head, such as 15 in Fig. 1, is not provided, but the outlet tube 14 itself may define the mouthpiece. The inlet for air may be defined by the outlet tube, the latter being sufficiently wide to permit sucking of air into the chamber. In this case, a mouthpiece may be provided having an inner outlet tube surrounded by venting, as shown in Fig. 7.

It is envisaged that a nebuliser may be

100 105 constructed according to the invention for use in an incubator.

The nebuliser may also be usable in non-medical fields, for example, for providing a fine spray in a greenhouse for dispersing an insecticide.

**CLAIMS**

1. Medical nebulising apparatus, comprising a housing including a chamber provided with a reservoir for material to be nebulised and having an air inlet, the housing having an outlet portion for nebulised material and a passage for nebulised material between the chamber and the outlet portion, and nebulising means in the form of a driven rotatable member for effecting nebulisation, the rotatable member having its path of rotation passing through the reservoir to pick up material, the passage communicating with the chamber

110 115 at a port radially spaced from the path of rotation and positioned in the path of particles flung from the rotatable member, and the chamber being shaped to direct particles to the port in an air stream centrifugally generated by the rotatable member.

2. Medical nebulising apparatus according to Claim 1, wherein the rotatable member is a disc pivotally mounted approximately at its centre and the chamber has a generally circular section generally perpendicular to the axis

120 125

130

of rotation of the rotatable member.

3. Medical nebulising apparatus according to Claim 2, wherein the rotatable member comprises a pair of closely spaced generally parallel discs mounted on a common axis of rotation.

4. Medical nebulising apparatus according to Claim 2 or 3, wherein the reservoir is defined by a narrowed portion of the chamber 10 opposite to the port, which is in the peripheral wall of the chamber, and the passage joining the chamber tangentially.

5. Medical nebulising apparatus according to any preceding Claim, wherein the air inlet 15 is in a wall of the chamber and its effective area is selectively variable.

6. Medical nebulising apparatus according to Claim 5, comprising a shutter, the wall of the chamber and the shutter being provided 20 one with a pointer and the other with a scale for indicating selectable positions of the shutter.

7. Medical nebulising apparatus according to any preceding Claim, wherein the rotatable 25 element is unbalanced to produce vibrations in the reservoir.

8. Medical nebulising apparatus according to any preceding Claim including particles in the reservoir incapable of nebulisation in the 30 apparatus to assist break up of material where the latter is powder.

9. Medical nebulising apparatus according to any preceding Claim including a baffle arrangement to assist return of larger particles 35 to the chamber, so as to control the size of particles of material in the air stream to a maximum of  $30\mu$ .

10. Medical nebulising apparatus according to any preceding Claim, wherein the passage 40 is defined by a first portion leading from the chamber and a second portion generally perpendicular thereto and leading to the outlet portion.

11. Medical nebulising apparatus according to Claim 10, wherein the first portion is in 45 two separable parts to permit filling of the reservoir through said port.

12. Medical nebulising apparatus according to Claim 10 or 11, including one or more 50 vents in the second portion or in the outlet portion.

13. Medical nebulising apparatus according to any preceding Claim including an electric motor for driving the rotatable member 55 and holding means for holding an electrical storage cell for operating the motor.

14. Medical nebulising apparatus according to Claim 13, wherein the motor and said holding means are provided in a casing detachable from the housing, and a splittable shaft 60 between the electric motor and the rotatable member.

15. Medical nebulising apparatus constructed substantially as herein described with 65 reference to Figs. 1 to 4, or Figs. 5 and 6, or

Figs. 7 and 8 of the accompanying drawings.

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